

Method and device for improving hearing aid fitting

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AREA OF THE INVENTION

The invention relates to the field of hearing aids and particularly to the fitting of hearing aids to the need of hearing-impaired individuals.

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BACKGROUND OF THE INVENTION

Usually the fitting of a hearing aid involves the adjustment of the transfer characteristics of the hearing aid signal path to the actual hearing loss of the individual. The hearing loss is usually determined in an audiometry test, which is well known in the field. Having made a first setting of the hearing aid signal path according to the actual hearing loss, a fine-tuning of the hearing aid transfer function is most often performed. This usually involves the presentation of test sounds, which may be presented by the hearing aid professional or as a part of the fitting software program, where the sounds are presented to the individual either alone or together with a visualization of the situation from which the sound originates. The hearing professional must in this process rely completely on the response from the hearing impaired in order to evaluate the actual settings. This may be a cumbersome process, especially in connection with first time hearing aid users.

25 Moreover in the fitting situation a need exists for increased user involvement in the actual technical fitting process, which is desirous in order to make the individual comfortable and feel secure about the situation and in order to achieve the best possible result in the fitting process.

30 The objective of the present invention is to provide a method, a system, a device and a software, which may provide improvement to the fitting situation in respect of the above mentioned shortcomings.

CONFIRMATION COPY

SUMMARY OF THE INVENTION

According to the invention the first aspect of the objective is achieved by means of
5 the method defined in claim 1.

By visualizing the input and/or the hearing aid transfer function relative to the
hearing threshold of the individual, the hearing professional will be able to evaluate
whether the hearing impaired should be able to recognize the input or not.
10 Furthermore by simulating how the hearing aid in its actual setting will process the
measured input and visualize this into a simulation or measurement of the patients
residual dynamic range, the hearing care professional can evaluate whether the
hearing impaired should be able to tolerate the input or not. Furthermore by
visualizing for the hearing impaired individual the input and the hearing aid transfer
15 function or the hearing threshold of this individual, he or she will obviously to a
significantly higher degree be involved in the fitting process and actually be able to
see, real-time or with a insignificant delay, what can and cannot be heard, and hereby
enter into a more active dialog with the hearing aid professional during the fitting
process. This inherently results in a fitting result that is improved compared to the
20 method hitherto used. Hence there is obviously an improvement in the fitting
situation and furthermore the possibility of reducing the time consumption in the
fitting process while at the same time achieving the same or an even better result of
the fitting.

25 The dependent claims 2-4 depict preferred embodiments of the method.

When at least two displays are provided for display of information to a patient and to
a hearing professional the patient may be involved in the fitting process in a
convenient manner. Preferably a selected information is provided at the patient
30 screen to avoid confusion.

The display update rate is preferably less than 1 second, preferably more than 0,1 second and less than 0,4 second. Hereby both the patient and the hearing professional may obtain the necessary information in a close to real-time manner.

- 5 Further the actual microphone input, the amplification characteristics, the simulated output, the microphone output, the UCL, the MCL or the MCR could be displayed in the same X-Y display. This add further information to the fitting situation.

According to the invention the second aspect of the objective is achieved by means
10 of the system as defined in claim 5.

By such system the same advantages as mentioned in connection with the method may be achieved.

- 15 Dependent claims 6-8 depict advantageous embodiments. The advantages correspond to those in connection with claims 2-4.

According to the invention the third aspect of the objective is achieved by means of the device as defined in claim 9.

20 By such device as a part of a system as described above for performing the method according to the invention the same advantages as mentioned in connection with the method may be achieved.

- 25 Advantageous embodiments are depicted in claims 10-12. The advantages correspond to those in connection with claims 2-4.

According to the invention the fourth aspect of the objective is achieved by means of the software as defined in claim 13.

30 By such software as a part of a system as described above for performing the method according to the invention the same advantages as mentioned in connection with the method may be achieved.

Advantageous embodiments are defined in the dependent claims. The advantages correspond to those in connection with claims 2-4.

The invention is described more detailed in the following description of a preferred embodiment with reference to the drawing.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 depicts a system comprising a hearing aid and a fitting device with screen where a hearing threshold is displayed and where simultaneously the level of a hearing aid output signal is displayed;

FIG. 2 is a more detailed presentation of a screen where the output is shown.

DESCRIPTION OF A PREFERRED EMBODIMENT

From FIG. 1 the system according to the invention appears in a schematic form. The system comprises a hearing aid, which is connected to a fitting device. The fitting 20 device comprises a hearing aid interface unit and a computer with a screen. The computer has in its memory a dedicated fitting software allowing adjustment of parameters in the hearing aid controlled by the computer or the hearing professional handling the computer.

From FIG. 2 the screen display appears where the hearing loss of the patient is displayed and where simultaneous the input, the amplification characteristics, the simulated output and/or the microphone output is displayed in the same coordinate system. Combinations of two or more of these parameters may be chosen for simultaneous display.

For the purpose of facilitating the fitting process a patient display could be provided, where this in order to avoid misunderstanding could display to the patient only the

data relevant for the patient and where the hearing aid professional could have a second display with full display of all data relevant to the fitting process.